

research article

Prognostic role of diffusion weighted and dynamic contrast-enhanced MRI in loco-regionally advanced head and neck cancer treated with concomitant chemoradiotherapy

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Background. In the study, the value of pre-treatment dynamic contrast-enhanced (DCE) and diffusion weighted (DW) MRI-derived parameters as well as their changes early during treatment was evaluated for predicting disease-free survival (DFS) and overall survival (OS) in patients with locoregionally advanced head and neck squamous carcinoma (HNSCC) treated with concomitant chemoradiotherapy (cCRT) with cisplatin.

Patients and methods. MRI scans were performed in 20 patients with locoregionally advanced HNSCC at baseline and after 10 Grays (Gy) of cCRT. Tumour apparent diffusion coefficient (ADC) and DCE parameters (volume transfer constant [K_{trans}], extracellular extravascular volume fraction [v_e], and plasma volume fraction [V_p]) were measured. Relative changes in parameters from baseline to 10 Gy were calculated. Univariate and multivariate Cox regression analysis were conducted. Receiver operating characteristic (ROC) curve analysis was employed to identify parameters with the best diagnostic performance.

Results. None of the parameters was identified to predict for DFS. On univariate analysis of OS, lower pre-treatment ADC ($p = 0.012$), higher pre-treatment K_{trans} ($p = 0.026$), and higher reduction in K_{trans} ($p = 0.014$) from baseline to 10 Gy were identified as significant predictors. Multivariate analysis identified only higher pre-treatment K_{trans} ($p = 0.026$; 95% CI: 0.000–0.132) as an independent predictor of OS. At ROC curve analysis, pre-treatment K_{trans} yielded an excellent diagnostic accuracy (area under curve [AUC] = 0.95, sensitivity 93.3%; specificity 80 %).

Conclusions. In our group of HNSCC patients treated with cisplatin-based cCRT, pre-treatment K_{trans} was found to be a good predictor of OS.

Key words: dynamic contrast-enhanced MRI; diffusion-weighted imaging; overall survival; squamous cell head and neck cancer; concomitant chemoradiotherapy

Introduction

Head and neck squamous carcinoma (HNSCC) is the seventh most commonly diagnosed cancer and the sixth most common cause of cancer death worldwide.¹ In a significant portion of patients with loco-regionally advanced disease, platin-based concomitant chemo-radiotherapy (cCRT) is the mainstay of treatment.^{2,3} However, current

treatment options remain suboptimal, since around 50% of patient experience tumour recurrence^{4,5} with the pathohistological evidence of residual regional lymph node metastases in up to 26% of patients with clinically determined complete response after cCRT.⁶ In addition, the reported 5-year overall survival (OS) rates are still well below 50%.⁷ In this scenario, improving prognostic stratification either before or early during cCRT would allow for pos-

sible modification of treatment regime in order to improve clinical outcomes and survival rates.

Multi-parametric imaging with functional imaging techniques has recently been used to evaluate biological properties of malignant tumours as changes at a cellular level typically occur prior to morphological changes. CT perfusion (CTP) has already been reported to provide a valuable information on tumour vascularity.⁸⁻¹⁰ In recent years, diffusion-weighted (DW) MR imaging (MRI) and dynamic contrast-enhanced MRI (DCE) have been used for assessing tumour biology and to predict tumour response and survival rates in patients with HNSCC. DWI is a widely used technique that allows for non-invasive measurement of the Brownian motion of water molecules by calculating the apparent diffusion coefficient (ADC) which reflects tumour cellularity and tissue microstructure.¹¹

Dynamic contrast-enhanced MRI (DCE-MRI) can assess the flow of blood through vessels in scanned tissues and therefore enables non-invasive characterization of tumour vascularity and perfusion.¹² Due to lack of standardization of data acquisition and analysis¹², the results of studies assessing the value of DCE-MRI derived parameters are still scarce and contradictory.¹³⁻¹⁵ In addition, studies addressing prognostic values of DCE-MRI parameters acquired early during treatment are lacking.

To the best of our knowledge, there is no data in the literature that would address the utility of combined DWI and DCE-MRI derived parameters before and early during treatment as prognostic factors for survival in HNSCC. Therefore, the objective of current study was to evaluate the prognostic value of imaging parameters from DWI and DCE MRI at baseline and early during treatment in loco-regionally advanced HNSCC patients treated with cisplatin-based cCRT.

Patients and methods

Patients and treatment

The study was approved by the National Medical Ethics Committee of the Republic of Slovenia (No. 22k/03/13) and written informed consent was obtained from all patients. Twenty patients with locally and/or regionally advanced (stages III-IVB) and histologically proven p16/HPV-negative SCC of the oro- or hypopharynx were enrolled in the study. p16/HPV status was assessed as described elsewhere.¹⁶ All patients were treated with cisplatin-based cCRT as recommended by the institutional multidisciplinary tumour board.

Patients were irradiated with a 6-MV linear accelerator photon beam using a concomitant boost intensity-modulated radiation technique. The dose to the primary tumour and enlarged lymph nodes was 70 Gy (gross tumour volume with a margin to compensate microscopic tumour extensions), whereas elective doses of 63 Gy (intermediate-risk volume - around larger nodes and non-palpable but radiologically suspicious nodes) and 56 Gy (low-risk volume) were applied for neck regions of probable microscopic disease in daily fractions of 2.0, 1.8 and 1.6 Gy, respectively, over 7 weeks. During radiotherapy, cisplatin in a dose of 40 mg/m²/week was concurrently administered. No antiangiogenic therapy was added to the protocol.

During therapy, toxicity was monitored on a weekly basis. After treatment completion, patients were examined for toxicity and tumour response every 2 to 3 months in the first and second year and every six months thereafter.

MR imaging protocol

All patients underwent three MR examinations with DWI and DCE-MRI: (1) 0–7 days before the treatment; (2) after 1 week (i.e., after the fifth fraction of radiotherapy, i.e. 10 Gy) and (3) 2.5–3 months after the completion of cCRT to assess radiological response to treatment.

MR imaging was performed on 3T MAGNETOM Trio, A Tim System (Siemens Medical Systems®, Erlangen, Germany) with a neck array coil. The diagnostic imaging protocol included axial T2-weighted sequences with short tau inversion recovery (STIR) from the base of the skull to aortic arch (TR/TE 5010/71 ms, TI 170 ms, flip angle (FA) 70°, receiver bandwidth 287 Hz/pixel, matrix size 256 × 256, slice thickness 3 mm, gap 0.3 mm and field of view (FOV) 18 × 18 cm). Axial slices that covered the entire primary tumour were selected for DWI and DCE-MR imaging.

DWI images were acquired in axial plane using pulsed spin-echo echo-planar image sequence (TR/TE 3600/86 ms, receiver bandwidth 1302 Hz/pixel, matrix size 180 × 192, slice thickness 5 mm, gap 1.5 mm, FOV 230 cm² and total acquisition time 5.04 min). Five different b-values (b = 0, 100, 200, 500 and 1000 s/mm²) were used with all diffusion-sensitizing gradients applied in three orthogonal directions to obtain trace-weighted images.

DCE-MRI was performed using 3D fast low angle shot (FLASH) sequence optimised for spatial and temporal resolution (TR/TE 5/1.16 ms, FA 15°, receiver bandwidth 490 Hz/pixel, matrix size 220

cm², slice thickness 4 mm, temporal resolution 4 s, total acquisition time 5 min. T1 mapping was used to convert signal intensities into gadolinium concentration. The T1 map was calculated from pre-contrast multiple flip angle images (6°, 10° in 15°). A k-space weighted image contrast algorithm was used to generate images with full spatial resolution of 128 x 128. Baseline images were acquired for 28 s. While the imaging continued, the gadobutrol (Gadovist®, Bayer HealthCare Pharmaceuticals) was administered intravenously in a dose of 0.1 mmol/kg body weight with a flow-rate of 3.5 ml/s followed by a 20 ml of saline flush with power injector.

Finally, post-contrast axial T1 weighted volumetric interpolated breath-hold examination (VIBE) sequences were acquired from skull base to aortic arch (TR/TE 3,26/1,26 ms, voxel size 1,1 x 0,9 x 1,5 mm with 4 mm averages, receiver bandwidth 640 Hz/pixel, matrix size 218 x 288 and FOV 250 cm²).

Imaging parameters analysis

Post-processing of all the images was performed at a workstation running commercially available software Olea Sphere® 3.0 MR Head & Neck expanded applications (Olea Medical®, La Ciotat, France). Before data analysis, motion correction algorithm was applied that allowed for pairwise in-plane (acquisition plane) rigid co-registration of all raw perfusion images of a given slice location with well-chosen reference image over time.

Quantitative DCE-MRI parameters were volume transfer constant (K_{trans}), extracellular extravascular volume fraction (v_e) and plasma volume fraction (V_p). The pharmacokinetic modelling was done on a pixel-by-pixel basis using the extended Tofts model - a two compartment model, which is suitable for any freely diffusible tracer. The equation modelling the contrast agent's concentration was the following¹⁷:

$$C(t) = v_p c_p(t) + K_{trans} c_p(t) \times \exp(-K_{ep} t)$$

where $C(t)$ is the tissue contrast agent concentration time course, V_p is plasma volume fraction, c_p is plasma contrast agent concentration, K_{trans} is the volume transfer constant and K_{ep} is the transfer function from extracellular extravascular space to the plasma space. The Arterial Input Function (AIF) for the pharmacokinetic analysis was derived from automatic selection of perfusion weighted image pixels selected in suitable arteries using a dedicated algorithm. The following multi-parametric

maps with K_{trans} , V_e and V_p were then obtained automatically.

Apparent diffusion coefficient (ADC) maps were computed by a single exponential fit using the DW signal intensity-b value curves.

ADC and DCE-MRI derived parameters as well as tumour volumes were measured at baseline and after 10 Gy. A radiologist (three years of experience in head and neck imaging) placed three regions of interest (ROIs) and analysed the multi-parametric ADC and DCE maps independently, with the T1 post-contrast images serving as the reference images. The ROIs were drawn manually on all imaging sections encircling solid-appearing portions of primary tumours and metastatic lymph node or nodal masses. Special attention was paid not to include necrotic and cystic areas (hyper-intense areas on STIR images), large feeding vessels and surrounding normal tissue.

Tumour volumes were calculated by manually encircling tumour borders on each T1 post-contrast sequence on all axial slices. Soft wear algorithm then calculated the volume by using the equation:

$$V = \text{encircled area} \times \text{section thickness}$$

Mean value of the selected ROIs from primary tumour was calculated for each parameter at each time point. Relative changes of the ADC and DCE-MRI parametric values as well as tumour volumes were calculated by dividing the mathematical difference of the corresponding parametric and tumour volume values after 10Gy and at pre-treatment by the pre-treatment parameter value for individual patient using the formula:

$$\Delta P_{10Gy} = \left[\frac{P_{10Gy} - P_0}{P_0} \right] * 100$$

where P represents any given parameter (ADC, K_{trans} , V_e , V_p or tumour volume), P_{10Gy} represents absolute value of the parameter after 10Gy, and P_0 absolute value of the pre-treatment parameter.

Outcome determination and statistical analysis

All data analysis and graphs were performed using statistical software SPSS 19.0 (IBM SPSS Statistics for Windows, Version 19.0. Armonk, NY: IBM Corp.). Shapiro-Wilk test and Levene test were used for normality testing and homogeneity-of-variance testing, respectively. The continuous variables are presented by median value and range. The relative changes in parameters between pre-treatment values and at 10 Gy are expressed in percentage (%). OS (event: death from any cause)

TABLE 1. The baseline clinical characteristics of all the patients

Patient	Sex	Age (yrs)	Tumour location	TNM	Stage
1	M	53	Oropharynx	T4aN1	IVA
2	M	67	Hypopharynx	T3N1	III
3	M	66	Hypopharynx	T3N2b	IVA
4	M	56	Oropharynx	T3N2b	IVA
5	M	49	Oropharynx	T2N2b	IVA
6	M	57	Oropharynx	T4aN2c	IVA
7	M	59	Hypopharynx	T4aN2b	IVA
8	M	60	Oropharynx	T3N2b	IVA
9	M	58	Oropharynx	T4aN2b	IVA
10	M	53	Oropharynx	T4aN2c	IVA
11	M	64	Oropharynx	T3N2c	IVA
12	M	56	Hypopharynx	T3N2b	IVA
13	M	65	Oropharynx	T2N2b	IVA
14	M	53	Hypopharynx	T4aN2c	IVA
15	M	66	Oropharynx	T3N2b	IVA
16	M	65	Oropharynx	T3N2a	IVA
17	M	46	Oropharynx	T3N3	IVB
18	M	67	Hypopharynx	T3N1	III
19	F	58	Oropharynx	T3N1	III
20	M	48	Hypopharynx	T3N1	III

Yrs = years

and DFS (event: persistent tumour after cCRT, loco/regional recurrence, systemic dissemination) was calculated from the first day of therapy using Kaplan-Meier curves. For assessment of prognostic value of MRI-derived parameters, patients were divided into two groups, according to treatment effect (DFS: without *vs.* with persistent tumour after cCRT or local/regional recurrence or systemic metastasis) or survival status at the end of observation period (OS: alive *vs.* death).

Non-parametric tests (Wilcoxon Signed Rank test, Mann-Whitney U test) were employed for comparative analysis of MRI-derived parameters under study. DFS and OS were plotted using the Kaplan-Meier method and significant predictors for survival outcomes were identified by univariate Cox regression analysis. All variables that reached the level of statistical significance in univariate analyses were entered into the multivariate Cox regression model, and stepwise forward selection was used to identify the independent predictors of DFS and OS. Receiver operating characteristic (ROC) curve analysis was applied to determine the discriminatory power of the ADC and DCE-MRI

parameters as well as tumour volume and clinical parameters for predicting survival rates. Area under curve (AUC) was computed and the optimal cut-off values were calculated by maximizing sensitivity and specificity. Two-tailed p values less than 0.05 were considered statistically significant.

Results

Patient data

All of the 20 consecutive patients (19 men, 1 woman; median age 58 years, range 46–67 years) with loco-regionally advanced HNSCC (oropharynx 13, hypopharynx 7) were free of systemic disease at presentation. The baseline clinical characteristics of the patients are listed in Table 1.

The median follow-up times of the entire study cohort and of the surviving patients were 27.2 months (range, 2.6–51.4 months) and 30.2 months (range, 18.2–51.4 months), respectively. In all patients, radiological complete tumour response to cCRT was determined 2.5–3 months post-therapy. Disease reappearance was diagnosed in 5 patients: 3 (15%) patients had recurrence at primary site, and 2 patients (10%) developed distant metastases (lungs). At the time of analysis, five patients (25%) were dead. Locoregional disease was the cause of death in three patients (with survival rates of 5.2, 10.6, and 22.9 months post-therapy), distant metastasis in one patient (14.1 months) and acute lower respiratory tract infection in the remaining patient (2.6 months, considered as treatment failure). A mean DFS was 38.9 months (2.6–51.4 months, 95% Confidence Interval [CI] 30.7–47.1). A mean OS time was 40.6 months (2.6–51.4 months, 95% CI 32.4–48.8). The 1- and 2- year DFS survival rates were 88.8% and 88.2% and for OS they were 84.4% and 73.8%.

Descriptive analysis of ADC and DCE-MRI derived parameters before and during treatment

For all the included patients, the pre-treatment values of ADC and DCE-MRI derived parameters K_{trans} , V_e and V_p were 0.81 (0.62–1.07) $\times 10^{-3}$ mm²/s, 0.48 (0.13–0.79) min⁻¹, 0.32 (0.15–0.64) and 0.17 (0.06–0.43), respectively. A statistically significant change from pre-treatment to 10 Gy was seen in all parameters: an increase of 22.5% (1.7 to 52.4%) in ADC ($p < 0.001$) and of 70% (73.2 to 357.14%) in V_p ($p = 0.015$) and a reduction of 50.3% (-93.4 to 179.2%) in K_{trans} ($p = 0.003$) and of 35.2% (-88.9

TABLE 2. Absolute values of DWI and DCE-MRI derived parameters and tumour volumes before treatment and their relative changes after 10 Gy (expressed as median and range) for the entire cohort of the patients and separately for alive and deceased patients at the end of follow-up

Parameters	The entire cohort of patients (n = 20, 100%)	Patients still alive at the end of follow-up (n = 15; 75%)	Deceased patients at the end of follow-up (n = 5; 25%)
Pre-treatment values			
ADC ($\times 10^{-3} \text{ mm}^2/\text{s}$)	0.81 (0.62–1.07)	0.76 (0.62–0.91)	0.96 (0.76–1.07)
K_{trans} (min^{-1})	0.48 (0.13–0.79)	0.57 (0.23–0.79)	0.22 (0.13–0.35)
V_e	0.32 (0.15–0.64)	0.32 (0.17–0.64)	0.22 (0.15–0.37)
V_p	0.17 (0.06–0.43)	0.15 (0.07–0.43)	0.35 (0.06–0.41)
Tumour volume (ml)	10.5 (2.6–54.9)	8.8 (2.6–44.55)	18.21 (6.6–54.9)
Relative changes after 10 Gy			
ΔADC	22.5% (1.7 to 52.4%)	25.0 (4.7 to 51.4)	9.2 (1.7 to 52.4)
ΔK_{trans}	-50.3% (-93.4 to 179.2%)	-60.0 (-93.0 to -43.2)	4.2 (-37.1 to 179.2)
ΔV_e	-35.2% (-88.9 to 126.8%)	-40.0 (-88.9 to 65.4)	-14.7 (-40. to 126.8)
ΔV_p	70% (73.2 to 357.14%)	92.9 (-18.6 to 357.2)	10.0 (-73.2 to 100)
$\Delta\text{Tumour volume}$	(-15.0%; -76.3 to 254.6%);	-14.0 (-76.3 to 254.6)	-19.6 (-37.7 to 114.72)

ADC = apparent diffusion coefficient; DCE-MRI = dynamic contrast-enhanced MRI; DWI = diffusion weighted imaging; Gy = gray; K_{trans} = volume transfer constant; V_e = extracellular extravascular volume fraction; V_p = plasma volume fraction; Δ = relative change in the parameter

to 126.8%) in V_e ($p = 0.024$). Pre-treatment tumour volume was 10.5 ml (2.6–54.9 ml). However, the change after 10 Gy from pre-treatment was not statistically different (-15.0%; -76.3 to 254.6%; $p = 0.823$) (Table 2).

The values of ADC and DCE-MRI derived parameters before treatment and the relative change of parameters after 10 Gy from baseline were com-

pared between patients alive at the end of follow-up and those who died (Table 2). Pre-treatment ADC ($0.76 \times 10^{-3} \text{ mm}^2/\text{s}$; $0.62\text{--}0.91 \times 10^{-3} \text{ mm}^2/\text{s}$) was significantly lower ($p = 0.042$) in patients which were still alive at the end of follow-up versus the patients who died ($0.96 \times 10^{-3} \text{ mm}^2/\text{s}$; $0.76\text{--}1.07 \times 10^{-3} \text{ mm}^2/\text{s}$). Alive patients also showed a significantly higher ($p = 0.002$) pre-treatment DCE-MRI

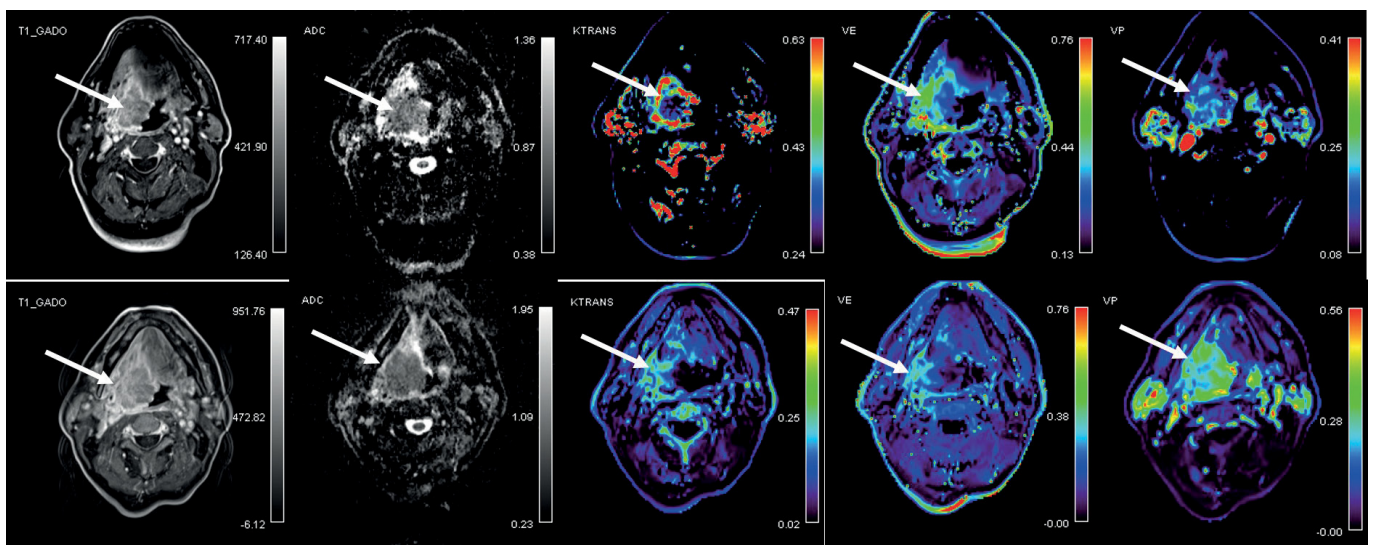


FIGURE 1. 58 year old patient with oropharyngeal squamous cell carcinoma (T4a N2b) who was alive at the end of follow up with overall survival of 41.1 months. Axial post-contrast T1 images, co-registered and corresponding apparent diffusion coefficient (ADC) maps and color-coded dynamic contrast-enhanced MRI derived volume transfer constant (Ktrans), extracellular extravascular fraction (Ve) and plasma volume fraction (Vp) maps in the area of the tumour (arrows) are shown. Top: before treatment; bottom: after 10 Gray of chemo-radiotherapy.

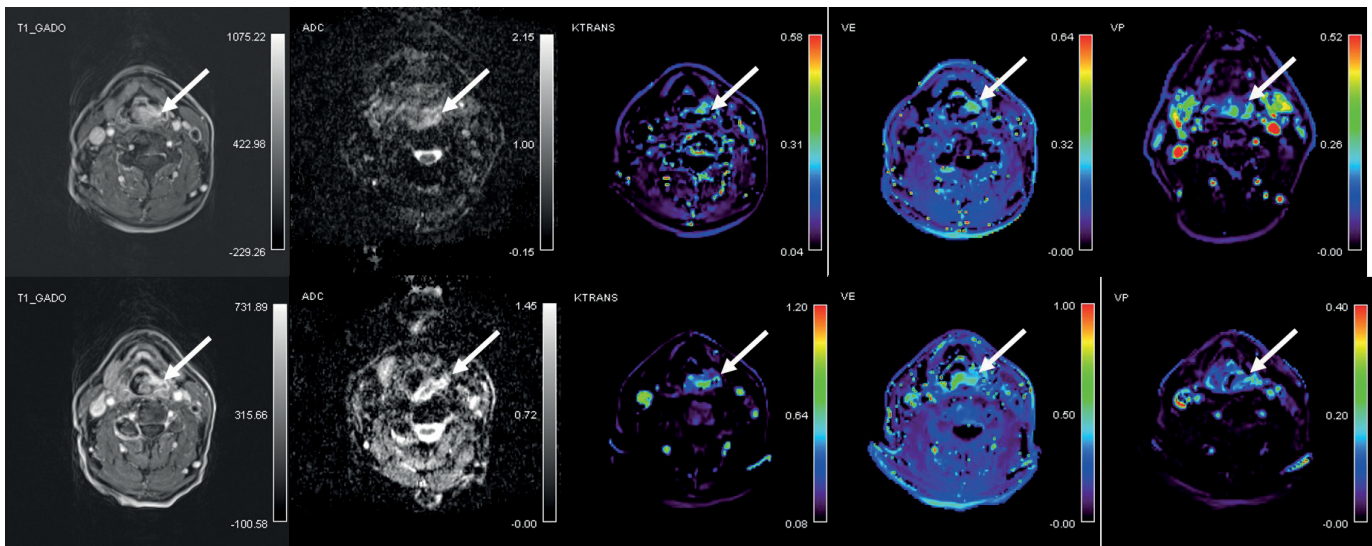


FIGURE 2. 65 year old patient with hypopharyngeal squamous cell carcinoma (T2 N2) who died 14 months of starting of chemo-radiotherapy due to disease relaps into the lungs. Axial post-contrast T1 images, co-registered and corresponding apparent diffusion coefficient (ADC) maps and color-coded dynamic contrast-enhanced MRI derived volume transfer constant (Ktrans), extracellular extravascular fraction (Ve) and plasma volume fraction (Vp) maps in the area of the tumour (arrows) are shown. Top: before treatment; bottom: after 10 Gray of chemo-radiotherapy.

derived parameter K_{trans} (0.57 min^{-1} ; $0.23\text{--}0.79 \text{ min}^{-1}$) compared with patients that died during follow-up (0.22 min^{-1} ; $0.13\text{--}0.35 \text{ min}^{-1}$). In addition, alive patients demonstrated a reduction in K_{trans} after 10

Gy from baseline (-60.0% ; -93.0 to -43.2%) whereas the patients who died showed no change or an increase in K_{trans} (4.2% ; -37.1 to 179.2%) ($p < 0.001$). There was no difference in the pre-treatment values of other perfusion parameters and tumour volumes ($p > 0.05$) nor in the relative changes from 10 Gy to baseline of ADC, V_e , V_p and tumour volume ($p > 0.05$). Illustrative examples of DW and DCE MRI images of alive and deceased patient at the end of follow up are shown in Figure 1 and 2, respectively.

On contrary, no significant difference was observed when values of all the functional parameters and tumour volumes were compared between patients that showed disease progression during follow-up and patients without disease progression ($p > 0.05$). However, in patients with noted disease progression there was a trend of larger pre-treatment tumour volume (14.0 ml ; $8.9\text{--}55.0 \text{ ml}$) compared to the group with disease controlled (6.6 ml ; $2.6\text{--}50.8 \text{ ml}$) ($p = 0.054$).

TABLE 3. Univariate analysis of risk factors associated with disease-free survival and overall survival rates ($n = 20$)

Parameters	Disease-free survival (p value)	Overall survival (p value)
Clinical parameters		
Age	0.338	0.556
Tumour location	0.396	0.752
Stage	1.000	0.198
Pre-treatment values of functional parameters and tumour volume		
ADC ($\times 10^{-3} \text{ mm}^2/\text{s}$)	0.856	0.012*
K_{trans} (min^{-1})	0.116	0.026*
V_e	0.754	0.293
V_p	0.165	0.342
Tumour volume	0.959	0.048*
Relative changes after 10 Gy of functional parameters and tumour volume		
ΔADC (%)	0.740	0.061
ΔK_{trans}	0.688	0.014*
ΔV_e	0.957	0.405
ΔV_p	0.672	0.077
$\Delta\text{Tumour volume}$ (ml)	0.495	0.486

* = significant predictor at univariate analysis; ADC = Apparent diffusion coefficient; K_{trans} = volume transfer constant; V_e = extracellular extravascular volume fraction; V_p = plasma volume fraction; Δ = relative change in the parameter

Univariate and multivariate Cox regression analysis

When assessing potential prognostic factors for DFS, none of them reached the level of statistical significance on univariate analysis (Table 3). Pre-treatment parameters that significantly influenced OS on univariate analysis were ADC ($p = 0.012$), K_{trans} ($p = 0.026$), and tumour volume ($p = 0.048$)

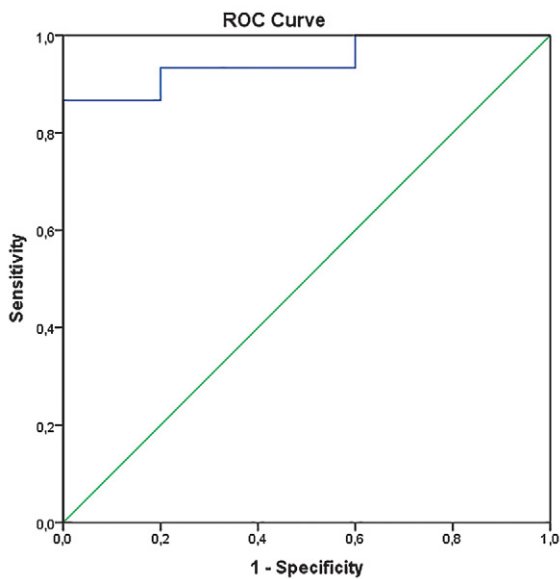


FIGURE 3. Receiver operating characteristic (ROC) curves for dynamic contrast-enhanced MRI (DCE-MRI) derived parameter K_{trans} (volume transfer constant) exhibiting area under ROC curve (AUC) of 0.95 with sensitivity 93.3% and specificity 80%. ($p = 0.003$).

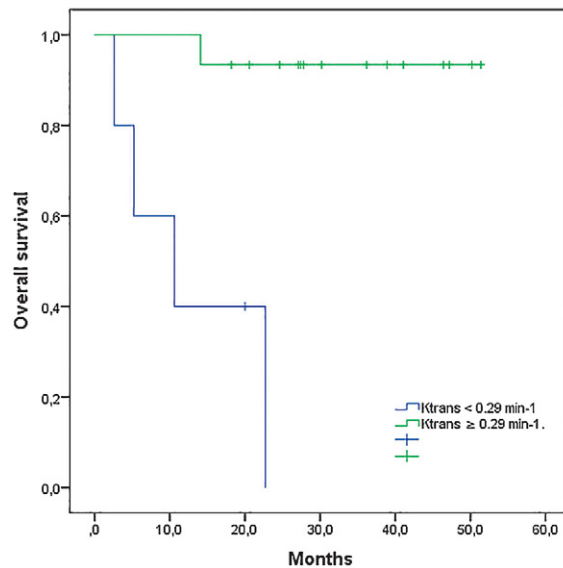


FIGURE 4. Kaplan-Meier estimates of overall survival in HNSCC patients (20) stratified according to pre-treatment DCE-MRI derived parameter K_{trans} (cut-off value of $\geq 0.29 \text{ min}^{-1}$, determined at ROC curve analysis).

DCE-MRI = dynamic contrast-enhanced MRI; K_{trans} = volume transfer constant; ROC = receiver operating curve

(higher K_{trans} and lower ADC and tumour volume were associated with longer survival). In addition, higher reduction in K_{trans} ($p = 0.014$) from baseline to 10 Gy was also identified as a significant prognosticator for OS but not also any of the clinical parameters (age, tumour location, TNM stage). Multivariate Cox regression analysis identified only higher pre-treatment K_{trans} ($p = 0.026$; 95% CI: 0.000–0.132) as an independent predictor of OS.

ROC curve analysis

When ROC curve analysis was performed, pre-treatment K_{trans} provided an excellent diagnostic accuracy with an area under curve (AUC) of 0.95 ($p = 0.003$; 95% CI: 0.85–1.00) and a sensitivity and specificity of 93.3% and 80.0%, respectively (Figure 1). The cut-off value for longer survival was set at $\geq 0.29 \text{ min}^{-1}$. In addition, a reduction in v_e after 10 Gy (survivors: median -40.0%, range -88.9% to 65.4%; deceased patients: median -14.7%, range -40.0 to 126.8%) yielded a good diagnostic accuracy with AUC 0.80 ($p = 0.055$; 95% CI: 0.569–1.000), sensitivity 73.3% and specificity 80.0%. Pre-treatment v_e showed only poor diagnostic usefulness accuracy (AUC 0.63), whereas other parameters failed to show any diagnostic accuracy (AUC < 0.6). When patients were grouped according to the K_{trans} cut-off value of 0.29 min^{-1} , the log rank test confirmed

a statistically significant difference in the length of OS between the two groups with mean survival of 48.9 months (95% CI: 44.2–53.6) in patients with pre-treatment $K_{trans} \geq 0.29 \text{ min}^{-1}$ and 12.8 months (95% CI: 4.1–21.4) in patients with pre-treatment $K_{trans} < 0.29 \text{ min}^{-1}$ ($p < 0.001$) (Figure 3).

Discussion

Our study showed that pre-treatment DCE-MRI derived parameter K_{trans} could serve as an independent prognosticator of OS. Thus, DCE-MRI may be used before and early during treatment to get insight into tumour vascularity and perfusion, which conditioned, among other biological factors, the response of the HNSCC to platin-based cCRT. The ability to identify specific pre-treatment parameters as well as their changes early during treatment could assist in identification of patients at higher recurrence and mortality risk. Therefore, re-consideration of existing treatment scenario might be indicated in such patients in order to maximize the chance of favourable outcome and to avoid unnecessary toxicity.^{18,19} In addition, more intensive surveillance could be performed in those individuals to detect eventual treatment failure in a timely manner.¹⁹

In present study, pre-treatment K_{trans} was found to be an independent prognostic factor for OS in both univariate and multivariate analysis with an excellent diagnostic accuracy in ROC analysis. DCE-MRI allows the analysis of vascular-related parameters in tumours and has primarily been used to predict treatment response and loco-regional control in HNSCC patients.²⁰⁻²⁵ Very few studies evaluated the role of pre-treatment DCE-MRI on the survival of HNSCC patients treated with cCRT. Chan and Chawla with co-workers found that lower pre-treatment K_{trans} is associated with poorer DFS and OS.^{21,26} On the contrary, two studies by Ng *et al.* failed to show the prognostic role of K_{trans} for survival in oropharyngeal HNC treated with CRT. Previous studies have already shown that higher pre-treatment K_{trans} values indicate better tumour response^{20,22} and loco-regional control to CRT.²⁴ K_{trans} is the volume transfer constant between the blood plasma and extracellular extravascular space and is a measure of both tumour blood flow and vascular permeability. Studies on different tumours found that K_{trans} correlates with the proliferating cell density and micro-vessel density (MVD).^{13,27,28} Both are used as markers of angiogenesis which is supposed to be the leading process for tumour growth, metastasis and radio-sensitivity.²⁹ The leading factor for stimulating angiogenesis is hypoxia, caused by structurally and functionally abnormal vessels and higher oxygen consumption by fast proliferating cells within the tumour micro-environment.³⁰ It is well-known that hypoxia enhances radio-chemoresistance through several mechanisms.³¹ Higher pre-treatment K_{trans} may therefore reflect greater tumour blood flow and vessels permeability, indicating enriched oxygenation that resulted in favourable radio-chemosensitivity status of the tumour.

Although the multivariate analysis failed to confirm an independent prognostic value of relative changes of K_{trans} , a higher reduction of K_{trans} after 10 Gy from baseline was found to be important for better OS in univariate analysis. Studies addressing the prognostic values on survival rates of DCE-MRI early during treatment are lacking. Kim *et al.* reported a reduction of K_{trans} in human head and neck tumour xenografts after only three days of RT or chemotherapy.¹³ Conversely, Baer *et al.* reported that patients with large-volume HNSCC with decreased K_{trans} after two weeks of therapy may have a shorter survival period.¹⁵ Aforementioned study by Kim *et al.* showed that reduction of K_{trans} correlates with the changes of both proliferating cell density and MVD and the authors postulated that

repopulation of RT-resistant endothelial cells after first days of CRT may be faster in more radio-sensitive tumours leading to lower permeability.¹³ Therefore, successful treatment leads to lower tumour perfusion and permeability, thus reflecting as a reduction of K_{trans} .

In addition, lower pre-treatment ADC was found to be a significant factor for longer survival at univariate analysis, but was not significant when multivariate analysis was applied. This is in agreement with Chan *et al.*²⁶ and Ng *et al.*³² who also found no significant prognostic value of pre-treatment ADC for 3-year OS in HNSCC treated with CRT. On the contrary, lower pre-treatment ADC was shown to be a consistent predictor of higher DFS of head and neck cancer to CRT.^{33,34} DW MRI is a quantitative imaging technique that measures diffusion of water molecules. Thus, in tissues with high cellularity (e.g. tumours), diffusion of water molecules is limited, showing as low ADC. Driessen *et al.* demonstrated that tumours with higher pre-treatment ADC had poorer prognosis due to lower cellularity and higher proportion of stroma that is a known independent poor prognostic factor.^{35,36} However, ADC value is probably affected by various physiologic parameters other than tumour cellularity and that needs to be explored further.³⁷

Our study has several limitations which have to be addressed. The main one is the small sample size and high number of parameters to analyse. However, our series is relatively homogeneous concerning primary tumour site and histological characteristics when compared to other studies conducted in HNSCC. This could explain why ADC or majority of DCE-MRI parameters failed to show any prognostic role when assessing OS and why none of the parameters was predictive for DFS. Larger prospective studies with higher number of patients and longer follow-up are needed in order to address the true prognostic role of DW and DCE-MRI derived parameters. Second, the DWI- and DCE-MRI-derived parameters were calculated as a mean value from the three most representative ROIs, delineated by only one radiologist. Therefore, no interobserver variability could be analysed, and appropriateness of ROIs marking procedure can also be questioned. Another limitation was that the DCE-MRI derived parameters and ADC were not compared to well-established histological biomarkers of angiogenesis (e.g. CD31 and Ki67 expressing cells). The last drawback can be attributed to the patient-specific AIF measurement as was used in our study: according to relevant studies, the use of a population-based AIF is

recommended due to most favourable repeatability.³⁸

In conclusion, the results of our study show that pre-treatment K_{trans} may serve as a biomarker of tumour angiogenesis. Therefore, DCE-MRI could play a role in determining prognosis of HNSCC patient treated with platin-based cCRT.

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